

Molecular recognition-controlled membrane disruption by a bis(crown ether) bola-amphiphile

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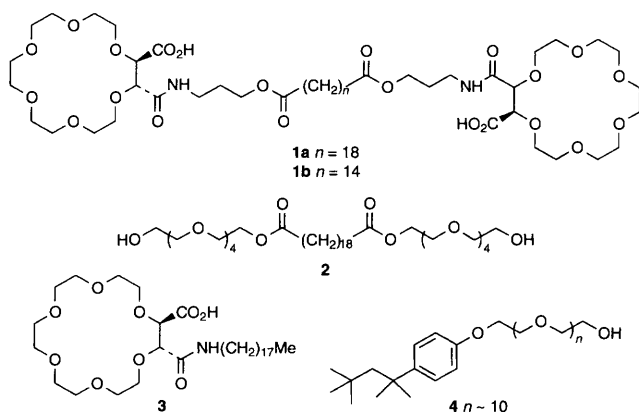
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Release of liposome-entrapped carboxyfluorescein is switched 'on' via molecular recognition of barium ion by a bis(crown ether carboxylate) bola-amphiphile.

Drug delivery using liposomes¹ relies on cell uptake of the liposome by fusion or phagocytosis.² Unfortunately, stabilized liposomes capable of specific cell targeting *in vivo* are resistant to these uptake mechanisms.³ A solution to this impasse would couple molecular recognition of the target to the release of liposome contents. This is one example of a general problem in signal transduction; specifically, how can a molecular binding event be amplified to a supramolecular membrane disrupting event? Consider the series of reports by Regen and co-workers⁴ on membrane disrupting systems based on bis(oligoethyleneoxide) bola-amphiphiles^{4a} and related polymeric derivatives.^{4b,c} There is considerable evidence that membrane disruption occurs *via* a U-shaped bola-amphiphile conformation.⁴ Perhaps molecular recognition-based control of membrane disruption might be achieved *via* U-shaped bis(crown ether) complexes⁵ in which formation of a 'sandwich' complex would create the required U-shaped conformation in the linking chain.

Here we report the behaviour of a bis(crown ether) bola-amphiphile system (**1a,b**) in comparison with **2**, an analogue of the compounds described by Regen,^{4a} and with **3**, a previously reported surfactant crown ether carboxylate.⁶ We expected **1a,b** to be less effective membrane disrupting agents than **2** due to repulsion of the charged head groups. However, the binding of a divalent cation in one of the crown ethers would favour approach of the head groups, thereby stabilizing a U-shaped conformation.

The synthesis of compounds **1a,b** follows from the structures. Dicarboxylic acids were converted *via* the acid chlorides to the bis(esters) of Z-protected 3-aminopropanol. Catalytic transfer hydrogenolysis of the protecting groups in formic acid⁷ afforded the stable bis(formate) salts. In basic solution, the free amine could be intercepted by the anhydride of (*R,R*)-1,4,7,10,13,16-hexaoxacyclooctadecane-2,3-dicarboxylic acid⁶ to give the target compounds in 35–45% yield over the three steps. Compound **2** was prepared following the published



procedure^{4a} starting from pentaethylene glycol in place of hexaethylene glycol.‡

Membrane disruption was assessed by monitoring the release of liposome-entrapped 5[6]-carboxyfluorescein (CF) following procedures described previously.⁴ Liposomes were formed in 0.1 M Na⁺CF or K⁺CF by a sonication–freeze–thaw method⁸ using 8:1:1 egg phosphatidylcholine–phosphatidic acid–cholesterol. The crude liposomes were sized through 0.45 μ m Nucleopore filters, and external CF was removed by gel filtration on Sephadex G-25 in a NaCl- or KCl-containing tris–HCl buffer. Aliquots of liposomes were incubated with varying amounts of **1–3** for 30 min, diluted with buffer, and the fluorescence emission intensity was recorded. The extent of release of entrapped CF was calculated from eqn. (1),

$$\text{CF release(\%)} = (I_{\text{obs}} - I_{\text{blank}})/(I_{\text{max}} - I_{\text{blank}}) \times 100 \quad (1)$$

where I is fluorescence intensity at 515 nm, and the subscripts denote the observed value for the sample (obs), the value for a blank sample (blank) and the maximum emission (max) for release of CF in excess Triton X-100. The extent of CF release as a function of the concentration of amphiphile is given in Fig. 1.

The behaviour of compounds **2** and **4** is qualitatively and quantitatively as expected.⁴ Both amphiphiles achieve full disruption at high concentration in either sodium- or potassium-containing CF solutions (0.14 M NaCl or KCl), and are unaffected by added calcium, strontium or barium chlorides (up to 0.01 M). Conversely, compound **1a** is notably inactive in a sodium-containing buffer system, shows a small tendency to disrupt in a potassium-containing system, but shows a marked

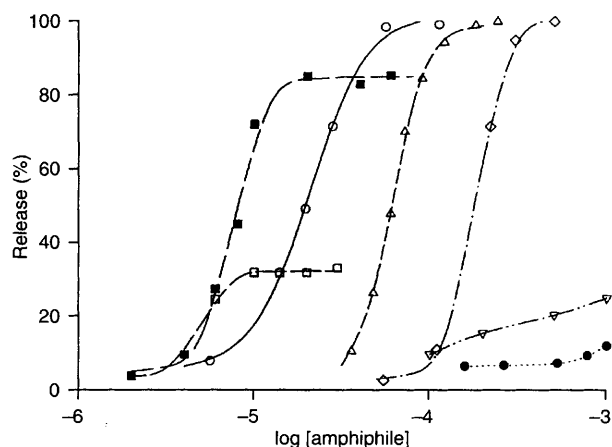


Fig. 1 Extent of carboxyfluorescein release as a function of amphiphile concentration after 30 min incubation of K⁺CF containing liposomes in 0.14 M KCl–tris–HCl buffer (pH 7.5) for **1a** (□), **1a** including additional 1 mM BaCl₂ (■), **1a** with NaCl in place of KCl (●), **1b** (∇), **2** (○) **3** (△) and **4** (◇). Experimental uncertainty in percentage release = ±5%. Curves for **2–4** in 0.14 M NaCl–Tris–HCl buffer, or buffers containing up to 0.01 M Ca, Sr or Ba chlorides are identical to those shown within experimental error (points omitted for clarity). Curves are calculated using non-linear fits to a 4 parameter logistic function.

ability to induce CF release in the presence of 1 mM barium added to either the sodium or potassium containing the buffer systems. The extent of disruption induced by Ba²⁺ never reaches the full extent of entrapped CF accessible to **2** or **4** (see below). Addition of 1 mM Ca²⁺ or Sr²⁺ also induces membrane rupture but the effect is less than with Ba²⁺ (Ca²⁺ 35%, Sr²⁺ 55% at log [1a] = -3.6). Compound **1b** is substantially less active than **1a**, as expected from Regen's results.^{4a} Comparison of **1a** and **3** reveals that cation selectivity is not an inherent property of crown ether surfactants; disruption by **3** is insensitive to Na⁺, K⁺ or additional alkaline earth salts.

The following features have been established. (i) The extent of release by **1a** is related to the fraction of unilamellar liposomes in the mixture. The uni-/multi-lamellar ratio was determined by a melittin assay.⁹ The liposomes for Fig. 1 were 88 ± 4% unilamellar. The **1a**:Ba²⁺ curve appears to approach this value as an asymptotic limit. To test this hypothesis, liposomes were prepared with a smaller unilamellar proportion (60 ± 3%); **1a** released 61 ± 5% of the entrapped CF in the presence of Ba²⁺. Similarly, an alternate liposome preparation containing 80 ± 4% unilamellar liposomes released 79 ± 5% of the entrapped CF. § (ii) The cation selectivity is a kinetic effect. In the Ba²⁺:**1a** system, >75% of the release eventually achieved occurs in the first 10 min, and the process is >95% complete within the 30 min incubation period. Without the Ba²⁺, 55% release requires 6 h, and >95% release requires >40 h. This slower release is still a factor of seven faster than a control without any added **1a**. (iii) The induced membrane disruption is related to molecular recognition of Ba²⁺ by the crown ether of **1a**. In addition to the cation selectivity, the extent of CF release as a function of the Ba²⁺:**1a** molar ratio appears as a hyperbolic curve. Analysis as a 1:1 binding isotherm yields an apparent binding constant of log *K* = 3.6 ± 0.3. This value is reasonable when compared to log β₁₁₀ = 5.5 ± 0.2 in 90:10 methanol-water solution for the butyl homologue of **3** plus Ba²⁺,¹⁰ or to an apparent interfacial association constant of log *K*_i = 3.0 ± 0.4 determined for Sr²⁺:**3** at a CHCl₃-H₂O interface.¹¹

A mechanism consistent with the results would involve partition of **1a** to the liposome and insertion into the outer leaflet. In the presence of K⁺ alone, the two crown ether head groups repel one another both sterically and electrostatically. This inhibits the formation of U-shaped loops in the connecting chain. The addition of Ba²⁺ allows formation of neutral 1:1 complexes in which the connecting chain is in a tight U-shaped loop leading to rapid membrane disruption. We are exploring

other systems based on the same mechanistic principle to establish the generality of this type of signal transduction.

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Footnotes

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‡ All new compounds were characterized by ¹H and ¹³C NMR, IR and electrospray mass spectra. Compound purity was established by analytical gel permeation chromatography and elemental analysis.

§ Extent of release is unrelated to size distribution: 88% release from a bimodal population distribution of liposomes [140 nm diameter (12%); 470 nm diameter (88%)], 61% release from a similar population distribution [170 nm diameter (15%); 540 nm diameter (85%)], but 79% release from a significantly different population distribution [140 nm diameter (30%); 400 nm diameter (70%)]. Size distributions were determined using a Nicomp 370 particle size analyser.

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